Imaging

- Imaging
 - Computed tomography

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Homework Assignment #7: Chapter 7: 2,3,9,10,11 due Monday, November 28, 2016

- Imaging
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Homework Assignment #7: Chapter 7: 2,3,9,10,11 due Monday, November 28, 2016 Final Exam, Wednesday, December 7, 2016, Stuart Building 213 2 sessions: 09:00-12:00; 13:00-17:00; (this may change)

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Homework Assignment #7:

Chapter 7: 2,3,9,10,11

due Monday, November 28, 2016

Final Exam, Wednesday, December 7, 2016, Stuart Building 213

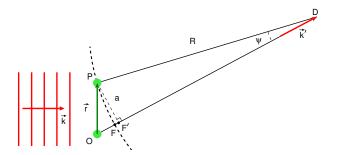
2 sessions: 09:00-12:00; 13:00-17:00; (this may change)

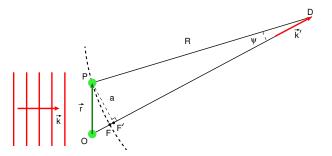
Provide me with the paper you intend to present and a preferred session for the exam

Send me your presentation in Powerpoint or PDF format before before your session

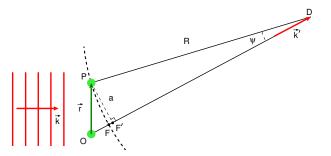
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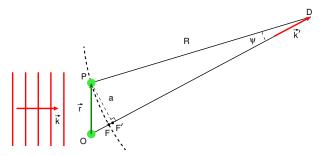


All imaging can be broken into a three step process



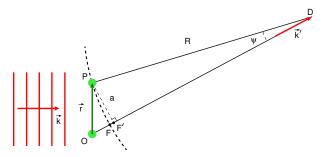
All imaging can be broken into a three step process

1 x-ray interaction with sample



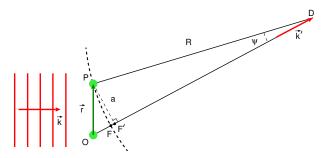
All imaging can be broken into a three step process

- 1 x-ray interaction with sample
- 2 scattered x-ray propagation



All imaging can be broken into a three step process

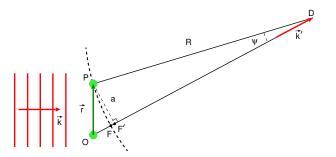
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All imaging can be broken into a three step process

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The scattered waves from O and P will travel different distances

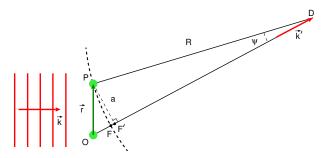


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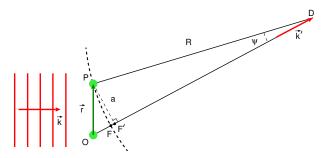
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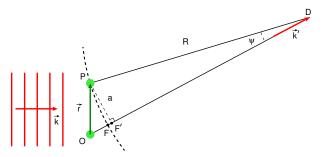
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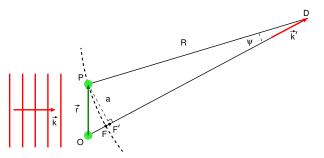
Since $\vec{k} \perp \vec{r}$, $\phi \approx \vec{Q} \cdot \vec{r} = \vec{k'} \cdot \vec{r}$

The path length difference corresponding to this phase shift is $\hat{k}' \cdot r = \overline{OF'}$

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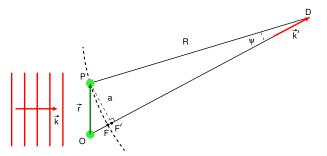


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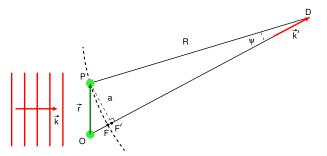
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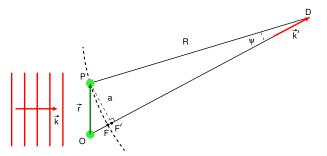
$$egin{aligned} \Delta &= R-R\cos\psi \ &pprox {\it R}(1-(1-\psi^2/2)) \end{aligned}$$

4



The path length difference computed with the far field approximation has a built in error of $\Delta = \overline{FF'}$ which sets a scale for different kinds of imaging

$$\begin{aligned} \Delta &= R - R \cos \psi \\ &\approx R(1 - (1 - \psi^2/2)) \\ &= R \frac{a^2}{2R^2} \end{aligned}$$

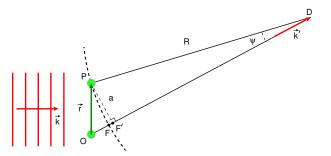


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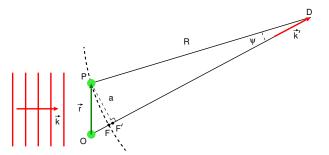
$$\approx R(1 - (1 - \psi^2/2))$$

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The path length difference computed with the far field approximation has a built in error of $\Delta = \overline{FF'}$ which sets a scale for different kinds of imaging a^2

$$\Delta = R - R \cos \psi \qquad \qquad R \gg \frac{a}{\lambda} \qquad \text{Fraunhofer}$$
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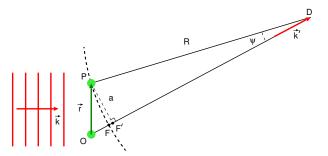


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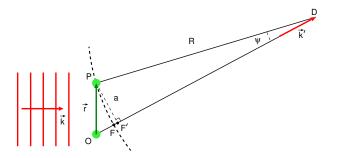
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$$= R \frac{a^2}{2R^2} = \frac{a^2}{2R} \qquad \qquad R \ll \frac{a^2}{\lambda} \qquad \text{Contact}$$

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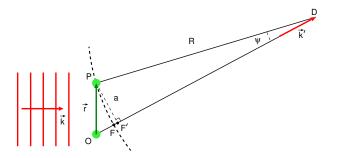
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Detector placement



If $\lambda = 1$ Å and the distance to be resolved is a = 1 Å, then $a^2/\lambda = 1$ Å and *any* detector placement is in the Fraunhofer (far field) regime

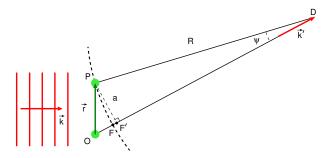
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if $a=\mu {\rm m},$ then $a^2/\lambda=10~{\rm mm}$ and the imaging regime can be selected by detector placement

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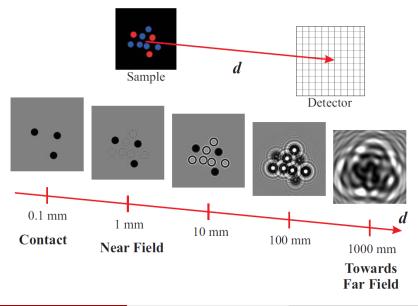
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if a=1 mm, then $a^2/\lambda=10$ km and the detector will always be in the contact regime

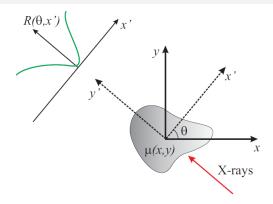
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Contact to far-field imaging



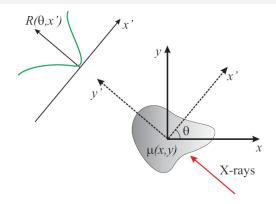
Radiography to tomography

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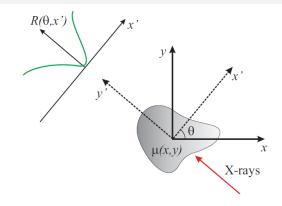
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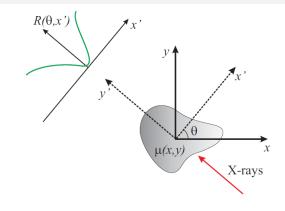
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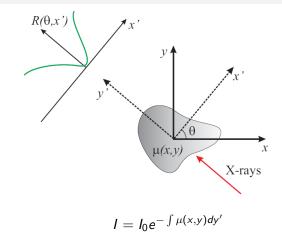
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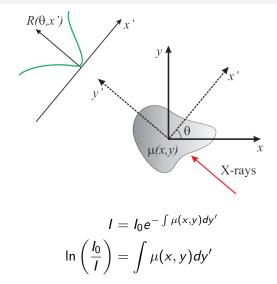
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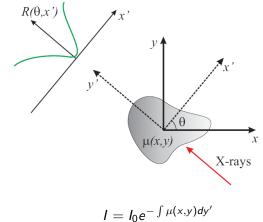
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$$\ln\left(\frac{l_0}{l}\right) = \int \mu(x, y) dy'$$

The radon transform $R(\theta, x')$ is used to reconstruct the 3D absorption image of the object numerically.

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Start with a general function f(x, y) which is projected onto the x-axis

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$$F(q_x,q_y) = \int \int f(x,y) e^{iq_x x + q_y y} dx dy$$

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$$F(q_x, q_y) = \int \int f(x, y) e^{iq_x x + q_y y} dx dy$$
$$F(q_x, q_y = 0) = \int \left[\int f(x, y) dy \right] e^{iq_x x} dx$$

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What is the relationship of the Fourier transform, $P(q_x)$, to the original function, f(x, y)? The Fourier transform of f(x, y) is $F(q_x, q_y)$ and by choosing $q_y \equiv 0$, we get a slice

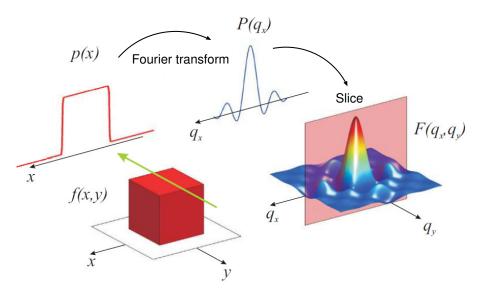
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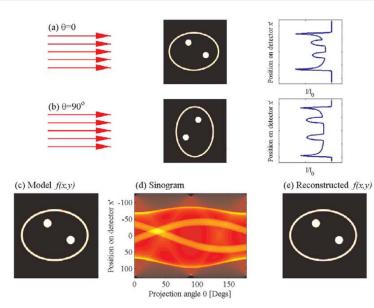
The Fourier transform of the projection is equal to a slice through the Fourier transform of the object at the origin in the direction of propagation

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Fourier transform reconstruction

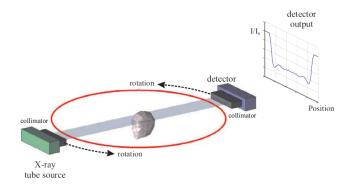


Sinograms



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Medical tomography

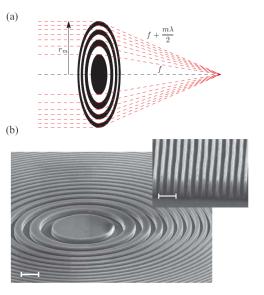




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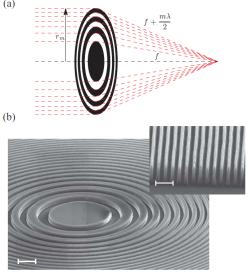
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The radius of the m^{th} zone is $r_m \approx \sqrt{m\lambda f}$



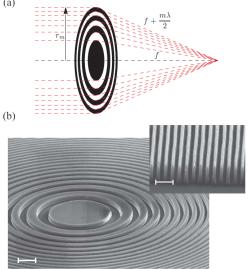
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The radius of the m^{th} zone is (a) $r_m \approx \sqrt{m\lambda f}$



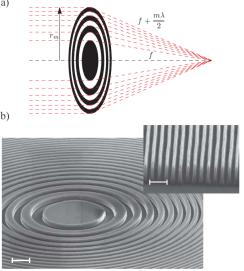
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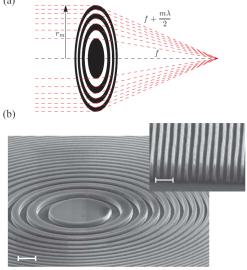
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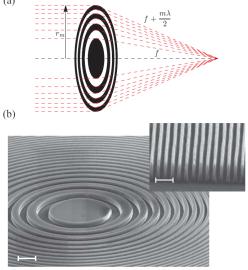
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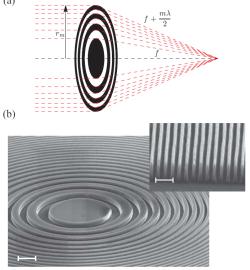
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$$D = 2r_M$$



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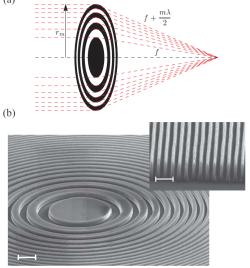
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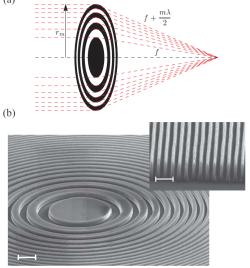
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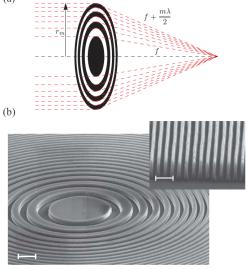
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$$D = 2r_{M} = 2\sqrt{M\lambda f}$$

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$$\Delta x = 1.22 \frac{\lambda f}{D}$$



The radius of the m^{th} zone is (a) $r_m \approx \sqrt{m\lambda f}$

$$\Delta r_{M} = \sqrt{\lambda f} (\sqrt{M} - \sqrt{M - 1})$$

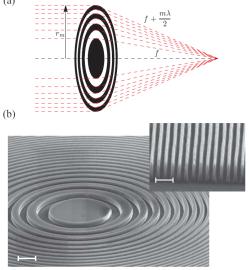
$$\approx \frac{\sqrt{\lambda f}}{2\sqrt{M}}$$

$$f = 4M \frac{(\Delta r_{M})^{2}}{\lambda}$$

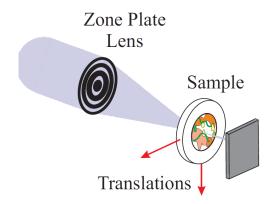
$$D = 2r_{M} = 2\sqrt{M\lambda f}$$

$$= 2\sqrt{M}\sqrt{\lambda f} = 4M\Delta r_{M}$$

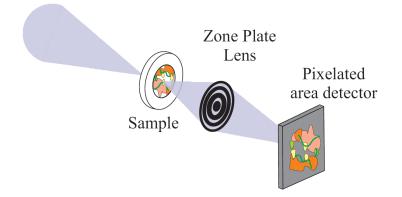
$$\Delta x = 1.22 \frac{\lambda f}{D} = 1.22\Delta r_{M}$$



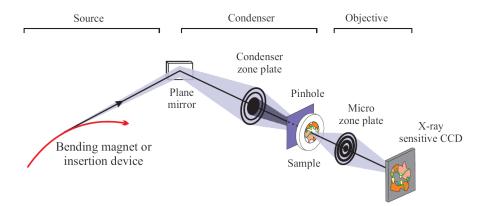
Scanning transmission x-ray microscope



Full field microscope



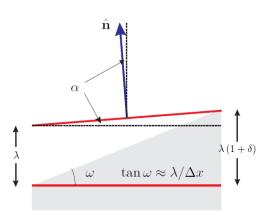
Transmission x-ray microscope



Angular deviation from refraction

When x-rays cross an interface that is not normal to their direction, there is refraction

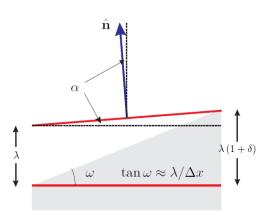
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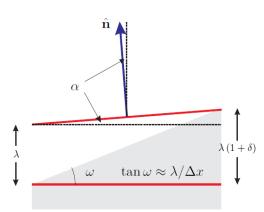
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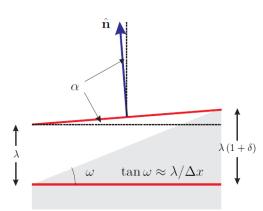
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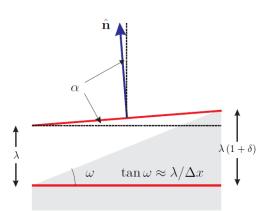
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$$\lambda_n = \frac{\lambda}{n}$$



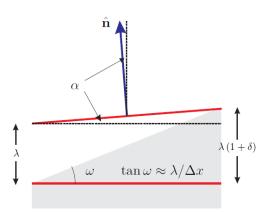
When x-rays cross an interface that is not normal to their direction, there is refraction

$$\lambda_n = \frac{\lambda}{n} = \frac{\lambda}{1-\delta}$$



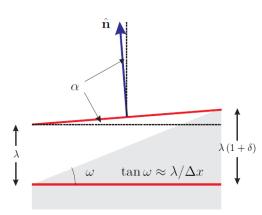
When x-rays cross an interface that is not normal to their direction, there is refraction

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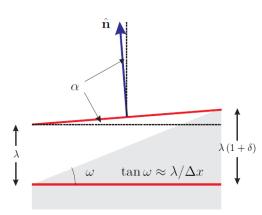
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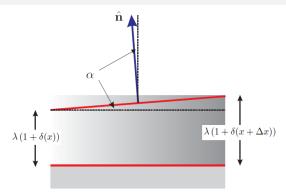
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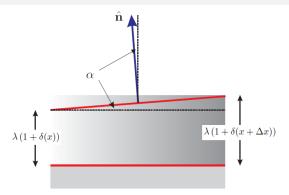
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In a similar way, there is an angular deviation when the material density varies normal to the propagation direction

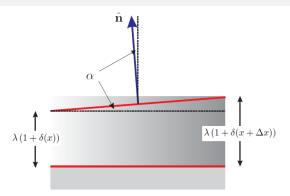


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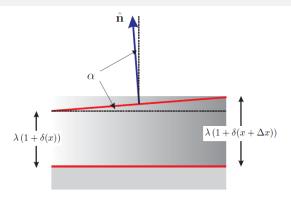
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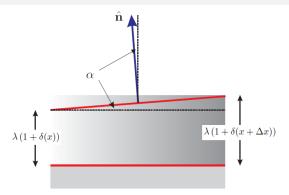
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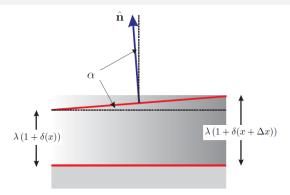


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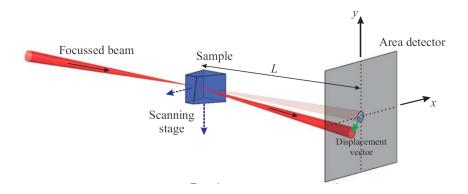
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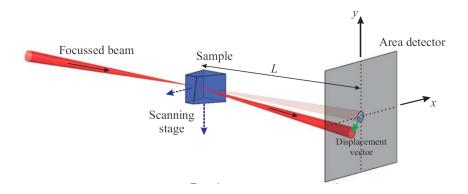
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By measuring the angular deviation as a function of position in a sample, one can reconstruct the phase shift $\phi(x, y)$ due to the sample by integration.

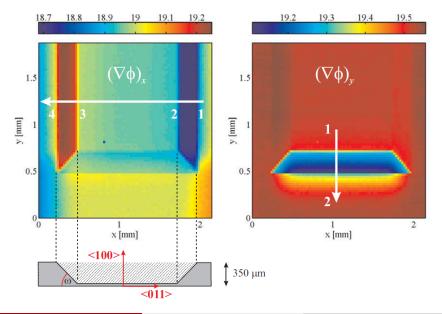
Phase contrast experiment



Phase contrast experiment

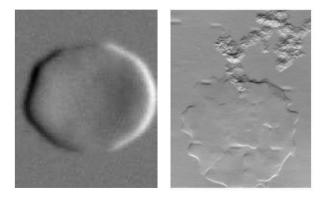


Imaging a silicon trough



C. Segre (IIT)

Imaging blood cells



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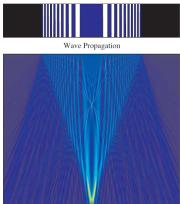
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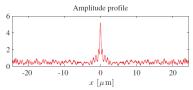
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Fresnel zone plates

Fresnel Zone Phase Plate

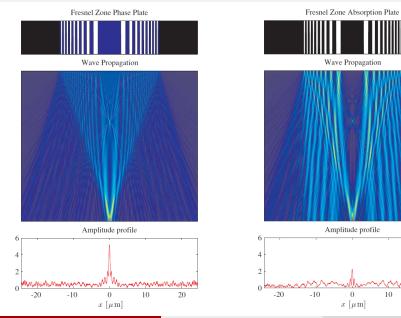




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Fresnel zone plates



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